

## **Armed Suture With Adhesively Attached Surgical Needle**

### **Field Of The Invention**

The present invention relates to armed sutures having surgical needles  
5 attached thereto and more particularly to such armed sutures wherein the needle is  
attached by an adhesive.

### **Background Of The Invention**

The attachment of surgical needles to suture with adhesives has been  
10 tried in the past. For example, U.S. Patent No. 3,799,169 to Beroff et al. and  
assigned to the present Assignee describes use of epoxy resin to bond a needle to a  
suture. When used with needles having a blind suture hole, epoxy is viscous,  
impeding the insertion of suture into the suture hole. Notwithstanding the prior art, it  
remains an objective to prepare armed sutures using adhesive attachment of the  
15 needle(s) which is easier to accomplish and provides greater pull strength and  
efficiency of production.

### **Summary Of The Invention**

The limitations of prior art, adhesively-attached, armed sutures are  
20 addressed by the present invention, which includes an armed suture having a needle  
with a suture hole formed therein. A suture has an end thereof inserted into the  
suture hole. An adhesive bonds the suture and the needle within the suture hole.

The adhesive has a viscosity when uncured permitting the suture to be inserted into the suture hole.

### **Brief Description Of The Figures**

5 Figure 1 is cross-sectional view of a surgical needle at an end to which suture is attached;

Figure 2 is a cross-sectional view like Fig.1, but with a reduced suture hole depth and coined end;

Figure 3 is a cross-sectional view of the needle of FIG. 1 but including a suture and  
10 adhesive material therein;

Figure 4 is a cross-sectional view of the needle of FIG. 2 but including a suture and adhesive material therein;

Figures 5a-5e are diagrammatic cross-sectional views of procedural steps conducted in accordance with the present invention for adhesively attaching a suture to a  
15 surgical needle;

Figure 6 is a cross-sectional view like Fig.1, but of a needle configured in accordance with an alternative embodiment of the present invention.; and

Figure 7 is a cross-sectional view like Fig.1, but of a needle configured in accordance with another alternative embodiment of the present invention.

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### **Detailed Description Of The Invention**

Figure 1 shows a surgical needle 10 with a suture hole 12 formed in an end 14 thereof by means of mechanical or laser drilling. The suture hole 12 has a

chamfered upper edge 16. As further described below, the configuration of the needle 10 shown in FIG. 1 is conventional except for the dimensions of the suture hole 12, viz., length L and diameter D, relative to the length and gauge of the needle.

In general, there are a few competing considerations as to suture hole 12

5 dimensions, viz., the larger the suture hole 12, the greater the potential surface area to which an adhesive in accordance with the present invention may bond.

Furthermore, the use of adhesives permits a larger suture hole 12, which can accommodate a range of suture sizes therein. From the stand point of drill wear (associated with drilling the suture hole 12) however, it is desirable for the depth of  
10 the suture hole 12 to be kept to a minimum.

Figure 2 shows a surgical needle 20 with a suture hole 22 formed in an end 24 thereof. Relative to the suture hole 12 of Figure 1, the suture hole 22 of Figure 2 has a reduced length L2 and an unchamfered upper edge 26. The upper edge 26 is "coined" or swaged inwardly to form a "bottle-shaped" suture hole 22  
15 having a reduced upper diameter D2 and a larger, lower diameter D3. This swaging effect may be accomplished by a Torrington Swaging unit obtained from Torrington Swager and Vaill End Machinery, Inc. of Waterbury, Connecticut.

Figure 3 shows the needle 10 of Fig. 1 with a suture 17 inserted into the suture hole 12 and retained there by adhesive 18. The adhesive 18 preferably  
20 has a low-viscosity to allow easy insertion of the suture 17 into the suture hole 12, i.e., by readily flowing between the suture 17 and the suture hole 12 as the suture 17 is inserted into the suture hole 12. A suitable adhesive is LOCTITE ® Product 4302, which is a low viscosity, two-part, UV-curable cyanoacrylate adhesive. It has a rapid

UV or visible light cure with a cyanoacrylate secondary cure mechanism. The use of adhesive 18 to attach the needle 10 to the suture 17 permits a variety of relative sizing of the needle 10 and suture 17 so joined. More particularly, the common mechanical method of swaging needles to sutures, i.e., without use of adhesives, requires close tolerances between the suture and needle. As a result only one size (diameter) suture made from a particular material may be used with only one size (diameter) suture hole. Since the adhesive 18 of the present invention bridges the gap between and bonds the suture 17 to the needle 10 (at the suture hole 12) a range of suture diameters and materials may be used with a single needle type (having a single set of suture hole 12 dimensions. This represents a significant advantage in that the number of different needles that must be manufactured, catalogued, maintained in inventory, processed, etc. may be greatly reduced, resulting in greater efficiency and substantial savings. From the standpoint of needle manufacturing, since the suture hole 12 may have a range of sizes and still be suitable for adhesive attachment, the needle 10 manufacturing costs may be reduced. For example, there may be a reduction in the number of different sized drilling apparatus used to produce the suture hole 12 in the needles 10. In addition, the drills (bits and apparatus) may be used longer because the manufacturing tolerances are not as close, so there is a reduction in wastage, testing, change outs and adjustments in needle drilling machines. Because the number of different needles is reduced, lot sizes can be increased, resulting in greater production with less setup. Because the suture hole 12 diameter can be larger than the suture 17, it is easier to insert the suture 17 into the suture hole 12. This advantage would be

expressed as a reduced "hole centering" requirement, which would be particularly important in an automated process. Because the needle 10 and suture 17 are attached by adhesive, no annealing step is required to reduce the stresses caused by swaging.

5                   Figure 4 shows a suture 27 inserted into suture hole 22 and affixed there by adhesive 28, which may be the same type of adhesive 18 as described above in reference to Figure 3. The coined upper edge 24 creates a bottle-shaped suture hole 22, such that when the suture hole 22 is filled with adhesive 28, the adhesive 28 also cures to a bottle-shape. This bottle-shaped adhesive 28 is  
10   mechanically locked into the suture hole 22. The mechanical interlock exhibited between the suture hole 22 and adhesive 28 allows the length of the hole 22 to be reduced while maintaining the same "pull strength," which is the tensile strength of the conjunction of the needle 20 with the suture 27. (When the pull strength is exceeded, the suture 27 would pull out of the suture hole 22, such as during  
15   destructive testing.)

                  Figures 5a through 5e illustrate an exemplary procedure in accordance with the present invention. In Figure 5a, a syringe 30 charged with adhesive 28 has a needle portion 31 that is inserted into the suture hole 22 of a needle 20. Figure 5b shows the adhesive 28 being injected into the suture hole 22. The use of a syringe  
20   30 or other graduated filling apparatus, such as a pipette, permits the controlled introduction of a suitable amount of adhesive 28 into the suture hole 22. It is desirable for the adhesive 28 injected into the suture hole 22 not to exceed an amount which would completely fill the suture hole 22 after the suture 27 is inserted.

That is, adhesive 28 overflow should be avoided. It is not necessary for the adhesive 28 to completely fill the suture hole 22 when the suture 27 is inserted, in that a lesser amount of adhesive 28 may provide sufficient attachment strength for a given application.

5                   After the predetermined amount of adhesive 28 is introduced into the suture hole 22, the syringe 30 is withdrawn, as shown in Figure 5c. The suture 27 is then inserted into the adhesive 28 deposited in the suture hole 22, as shown in Figure 5d. Figure 5e illustrates the irradiation of the adhesive 28 with UV, visible light or other electromagnetic radiation 33 to aid in the curing of the adhesive 28.

10   Depending upon the adhesive 28 used, radiation may not be required for the curing of the adhesive 28. The advantages of UV-curing adhesive 28 is that it may be dispensed in the non-viscous, liquid state to facilitate filling the suture hole 22. The adhesive 28 may then be partially or completely cured while the suture 27 is held in the adhesive 28, accomplishing attachment and allowing the attached suture 27 and

15   needle 20 to be released by the holder. The foregoing process may be accomplished entirely manually or be aided by fixtures which, e.g., hold the needle 20 for filing, hold the syringe 30 during the injection of adhesive into the suture hole 22 and hold the suture 27 and needle 20 while the adhesive 28 is irradiated. In addition, the process may be mechanized, such that all the foregoing steps are accomplished by

20   machines, robotically and automatically.

Instead of pre-filling the suture hole 22 with adhesive 28, the foregoing process may be varied by dipping the suture 22 into a reservoir of adhesive 28 and then inserting the adhesive-wetted end of the suture 27 into the suture hole 22.

When using low viscosity adhesives, the adhesive 28 into which the suture 27 is dipped may be partially cured to increase viscosity and slow the flow of adhesive down the suture 27.

As a further alternative, either of the foregoing processes, viz. pre-filling and dipping, may incorporate the use of a catalyst. For example, the LOCTITE® 4302 adhesive mentioned above utilizes cyanoacrylate as a secondary cure mechanism. Accordingly, the suture hole 22 can be coated with cyanoacrylate prior to filling with adhesive 28 in the pre-filling approach or, prior to insertion of the dipped suture, in the dipping approach. Further, the suture 27 can be dipped, painted or sprayed with the chemical curative, e.g. cyanoacrylate, prior to being dipped, or inserted in the adhesive 28.

Curing time (and pull-out strength) is effected by the intensity and duration of exposure to radiation, to the length of time between radiation curing and testing, by the use of a chemical curative, e.g. cyanoacrylate, and other factors, e.g., heat. In some instances, a first type of curing, e.g. a short exposure to visible or UV light may partially cure the adhesive, (flash it over) followed by a more complete cure attributable to time, chemical curatives, atmospheric moisture, and/or heat and other forms of radiation (microwave). It has been observed that sterilization of armed sutures in accordance with the present invention by heat and/or irradiation contributes to curing.

Figures 6 and 7 illustrate needles 40 and 50, respectively, which include grooves 43 and 53, respectively, to increase the mechanical interlocking of the adhesive 28 and the needles, 40, 50. It has been observed that increased

surface roughness in the area of the suture hole 12, 22, 42, 52 increases pull-out strength. This is evident when comparing the pull-out strength of finished vs. unfinished needles. Accordingly, methods for isolating the suture hole, e.g.; 12 from finishing, such as by using water or wax plugs are advantageous. As another  
5 alternative, the suture hole 12 of a finished needle can be roughened by acid etching, by mechanical processes, such as by reaming with a rough reamer, or by laser drilling. The foregoing features of the present invention are further exemplified and illustrated by the following examples:

#### 10 **Example 1**

Size 3-0 Ethilon and size 3-0 coated Vicryl sutures were used in this example. Both suture types were attached to unfinished 493962 needles, which have an nominal hole diameter of 14.5 mil. The 3-0 Vicryl was also attached to finished 522617 needles, which have a nominal hole diameter of 15.8 mil. The adhesive was applied  
15 using the suture dip method. The sample sizes varied for each set of pulls.

Each of the attachment types was pulled in varying sample sizes at less than 10 minutes from exposure and then at greater than 24 hours from exposure. The exposure times (to UV light) varied from 5 to 9 seconds.

The pull test averages were as follows:

<b>Suture – Needle Combination:</b>	<b>Within 10 Min. of Cure</b>	<b>24 Hours from Cure</b>
3-0 Ethilon – Unfinished 493962	0.64 lb	0.52 lb
3-0 Vicryl – Unfinished 493962	3.20 lb	4.90 lb
3-0 Vicryl – Finished 522617	0.60 lb	1.83 lb

This test confirmed the secondary curing effects of the LOCTITE 4302 adhesive with regard to the Vicryl suture.

### **Example 2**

5    Sizes 4-0, 2-0 and 1 coated Vicryl were used in this study. All three suture sizes were attached to 483947 needles, which have a nominal hole diameter of 24. 8 mil. The cure time for sizes 4-0 and 2-0 was 1 second, and for size 1 the cure time was 3 seconds. All attachments were performed using the syringe injection method of adhesive application.

10   For each suture size, n=12 samples were pulled immediately after curing, another n=12 were pulled after 30 minutes, and another n=12 were pulled after 24 hours.

All three suture sizes showed comparable initial cure strengths, as shown below.

Both the 4-0 and 2-0 attachments showed steady increases in strength over time, and achieved final pull strengths which met current in-process manufacturing

15   standards for that suture size.

<b>Vicryl Suture Size</b>	<b>Exposure Time</b>	<b>Immediate Pull</b>	<b>30 Min. from cure</b>	<b>24 hr. from cure</b>
4-0	1 sec.	0.71 lb	2.17 lb	3.07 lb
2-0	1 sec.	0.33 lb	2.17 lb	4.19 lb
1	3 sec.	0.54 lb	5.28 lb	5.14 lb

This example showed that the adhesive 4302 from LOCTITE does in fact achieve an improved attachment strength over time when used in needle/suture attachment. It

20   also showed that this adhesive process is capable of producing pull values higher

than current in-process requirements for these products, and that this type of attachment is effective regardless of hole size.

### **Example 3**

- 5 Two needle types were used in this example 483947 and 483966, both of which have a 24.8 mil nominal hole diameter. The 483947 needles were finished, and 483966 were unfinished.

Both needle codes were attached to size 1 Vicryl. The exposure time was 2 seconds and the pull testing (n=5) was performed one hour after exposure to the  
10 ultra violet light. The adhesive was applied by the syringe injection method.

The finished needle attachment averaged 3.64 lb and failed due to breakdown of adhesive-to-needle bonding, while the unfinished attachments averaged 10.84 lb and failed at the adhesive-to-suture bond.

<b>Needle Finish</b>	<b>Needle RMC</b>	<b>Pull Averages (n=5)</b>
Finished	483947	3.64 lb
Unfinished	483966	10.84 lb

- 15 The most likely explanation for the foregoing results is that the polishing process removes the inconsistencies found in the unfinished needle hole which help the adhesive form a mechanical bond. Trace amounts of silicone in the needle hole may also cause poor attachment to the finished needle.

#### **Example 4**

Size 3-0 coated Vicryl suture was used for this example.

Unfinished 493966 needles with a 24.8 mil hole were used in this example. To achieve the different hole depths, each needle was manually ground on the hole end until the depth corresponded to the required depth. Samples of these needles were attached with hole depths at nominal depth, 50 mil, 40 mil, and 30 mil. The cure time for each attachment was 3 seconds. Each of the samples were pulled in groups of n=12 immediately after attachment, at 30 minutes from the attachment and 24 hours after attachment. Another n=12 group from each set of samples was put through Ethylene Oxide sterilization (F cycle), then spent four days in "hot room" conditions, and were then pulled.

All four groups showed pull values of less than 1 lb. when pulled immediately after attachment. After 30 minutes, the pull strengths were more widely varied, but all values were significantly higher than the in-process manufacturing requirement of 2.5 lb. After 24 hours, each of the sample sets increased in strength by approximately 18 oz, on average. Following the sterilization process, which took about 3 weeks, each of the samples experienced another increase of approximately 12 oz, on average.

<b>Hole Depth:</b>	<b>Immediate Pull</b>	<b>30 min. from cure</b>	<b>24 hr. from cure</b>	<b>Sterilized</b>
.030"	0.72 lb	3.95 lb	5.20 lb	5.68 lb
.040"	0.68 lb	4.81 lb	5.90 lb	6.87 lb
.050"	0.80 lb	5.83 lb	7.07 lb	8.05 lb
Nominal	0.88 lb	6.00 lb	6.92 lb	7.68 lb

The 50 mil hole depth results were indistinguishable from the nominal hole depth of approximately 67 mil. With very few exceptions, all failures after the “immediate” pull were due to adhesive-to-suture bond failures, or suture breaks induced by the rough hole edges left by the grinding process used to achieve the experimental hole depths. This example shows that a reduction in hole depth down to 30 mil still provides enough surface area to produce sufficient pull strength on 3-0 coated Vicryl.

### **Example 5**

Size 2-0 Vicryl was used in this example, as it is the largest suture which was readily available and would fit in each of the reduced holes. The reduced hole needles were 483840, mechanically drilled, chamfered, straight needles (obsolete) which have a nominal hole diameter of 20.2 mil, but were measured in the lab at an average of 20.0 mil. The diameters of the ends of the needles were reduced using a Torrington Swaging unit. The attachment end of each needle was manually inserted into the swager to varying depths from about 0.400” to 0.420”. This caused hole collapse of anywhere from .0015” to .0055”. The resulting holes were then measured with pin gauges and separated into groups with upper hole diameters of 18, 17 and 16 mil (+/- .2).

Initially, samples of the unmodified 483840s and samples of the same needles reduced to an upper hole diameter of 18 mil (n=12 for both groups) were attached to the size 2-0 coated Vicryl. The adhesive was exposed to low intensity ultra violet light for three seconds, and the samples were pulled after approximately 65 hrs.

Later samples (n=4) of 17 mil and 16 mil reduced holes were attached and pulled according to the same description. The first two samples showed an increase in pull strength from 3.84 lb using the standard hole geometry to 4.94 lb using the 18 mil modified hole geometry. The 17 mil samples showed even more of an increase, to 6.02 lb, as shown in the chart below:

Top of Hole Reduction	Sample Size	Pull Average
Nominal	12	61.5 oz
.002"	12	79.0 oz
.003"	3	91.6 oz
.004"	4	25.0 oz

#### **Example 6**

Sizes 5-0, 6-0, 7-0 and 8-0 ProNova\* suture were obtained for this test. The needles used in the attachment were 521610 needles, which have a hole diameter of 7.5 mil. This hole is normally swaged with a size 5-0 suture but, consistent with our current method of testing, all sizes in this test were attached using the same hole diameter.

The "syringe injection" method of attachment was not appropriate in this case, as the hole diameter could not accept a syringe needle. Instead, the "suture dip" method was used.

Initially, ten samples using size 5-0 suture were attached and pull tested after approximately 30 minutes. The average of the resulting pull values was 123.5g (IPQA: 227g). Examination of the samples showed very low levels of adhesive filling.

Further investigation showed inadequate beading of the adhesive on the suture tip due to its low viscosity.

In order to achieve a satisfactory attachment, a small amount of adhesive was left exposed to the ambient atmosphere in an open reservoir for approximately 24 hrs. The resulting effect was a partial curing of the adhesive, and thus an increase in its viscosity. Noticeably higher levels of adhesive beading and filling of the attachment area were achieved.

ProNova* Suture Size	Pull Average	IPQA Required Average
5-0	207 g	227 g
6-0	112 g	170 g
7-0	84 g	90 g
8-0	95 g	-

Although adhesive filling of the attachment area was significantly improved using the partially cured adhesive, complete filling was still not achieved. All the low pulls in the test showed poor adhesive filling.

Trailers resulted from the use of the partially cured adhesive, as well. These were fine strands of adhesive which trailed from the attachment area and were a product of the combination of partial curing and suture dipping.

#### 15 **Example 7**

This example was conducted to explore briefly the effects of the *LOCTITE*® accelerator 7109 and activator 7113 used in conjunction with *LOCTITE*® 4302 light curable adhesive. According to *LOCTITE*® product information, the 7109 and 7113 products significantly alter the secondary moisture curing properties of 4302

adhesive. Both products induce faster curing, but there is some sacrifice of overall strength with the 7109.

Size 4-0 coated Vicryl suture was used. The suture was attached to 483947 needles, which have a 24.8 mil nominal hole diameter. The accelerators were applied by spraying the fluids toward the hole end of the needle from approximately six inches away. The needles were sprayed three at a time to avoid problems with accelerator evaporation. The suture was then attached using a syringe injection method.

This example compares pull strength when curing is a) unaccelerated or accelerated with b) 7109 or c) 7113 used as an accelerator. Seven samples of each type were attached and pulled after 30 minutes.

The attachments resulting from the use of accelerator 7109 showed the highest pull results, averaging 3.71 lb. For reference, in the Vicryl Time Study, the pull average after 30 minutes was just 2.17, the highest pull average reached (n=12) after 24 hrs was 4.19 lb.

The resulting averages were as follows:

Using 7109	Using 7113	Unaccelerated
3.71 lb.	3.67 lb.	1.45 lb.

The use of accelerators caused some amount of difficulty in manual attachment, due to the rapid cure of the adhesive in contact with the accelerators. Also, shallow suture insertions were observed in some of the accelerated samples. These

*LOCTITE* ® accelerators can induce faster cures in the 4302 adhesive. In those cases which showed shallow suture insertions some curing took place in the bottom of the needle hole before the suture could even be inserted.

It should be understood that the embodiments described herein  
5 are merely exemplary and that a person skilled in the art may make many variations and modifications without departing from the spirit and scope of the invention as defined in the appended claims. For example, while an exemplary adhesive<sup>18</sup> has been identified as *LOCTITE*® 4302, other adhesives, such as *LOCTITE*® 4303,  
4304 and 4305, could be employed. All such variations and modifications are  
10 intended to be included within the scope of the present invention as defined in the appended claims.